IOT-BASED WRIST BAND CONTROLLED WHEELCHAIRFORPARALYZEDPATIENTS

Kalaiselvan S

ComputerScienceandEngineering KarpagamcollegeofEngineering Coimbatore India 20p320@kce.ac.in

Santhosh G

ComputerScienceandEngineering Karpagamcollegeof Engineering Coimbatore India 20p343@kce.ac.in

Arunprasanth B

ComputerScienceandEngineering Karpagamcollegeof Engineering Coimbatore India <u>21p701@kce.ac.in</u>

Tharun Kumar

A ComputerScienceandEngineering Karpagam college of Engineering Coimbatore India 21p706@kce.ac.in

Mr.Ramaraj S ComputerScienceandEngineering Karpagm college of Engineering Coimbatore,India ramaraj.s@kce.ac.in

Abstract- The wheelchair stands out as a widely embraced assistive technology for individuals with motor impairments, offering both environmentally friendly mobility and comfort. Despite its widespread use, the traditional wheelchair's operational method presents challenges for those with finger- related issues. However, the conventional wheelchair's

operational method remains inconvenient for individuals facing finger problems, as these inputs are crucial for controlling the wheelchair's movement-forward, left, right, or backward. This system empowers users to move independently without relying on external assistance. To enhance obstacle detection safety, an systemhasbeenincorporated into the overall scheme, consisting of sensor devices and a fog server. If an obstacle is detected, an LCD provides a visual indication. The scheme not only ensures continuousmonitoringofvitalsignsbutalsoincorporatestested indicatorstodeterminetemperaturelevels, forminganintegrated locator system. The study's findings demonstrate that participantswereabletonavigatethewheelchaircomfortablyto their destination without collisions. The experimental results highlight the high accuracy of the proposed approach and its potentialinaddressingissuesrelatedtofingerdependenciesand hand fatigue.

Keywords-Sensor, Automation, IOT, MicroController.

I.INTRODUCTION

Inrecentyears, there has been a significant surge in the aging population, presenting a formidable social and economic challenge for the 21st century. Advances in medicine and public health services have substantially increased life expectancy, with projections indicating a doubling of the proportion of individuals aged 60 and above from 10% to 22% in the next 50 years. Many older adults prefer aging in place, maintaining their independent lifestyles, despite the associated highrisks. Alarmingstatistics from the Centers for Disease Control and Prevention (CDC) reveal that one in three adults aged 65 and older experiences a fall each year, with 61% of these falls occurring at home and resulting in 10,000deaths.Swiftassistancepost-fallsignificantlyreduces hospitalization risk by 26% and lowers the mortality rate by 80%. Inresponse to the sechallenges, various supportive

technologies and systems have emerged to monitor the activities of the elderly at home, aiming to support independent living and mitigate the premature need for institutionalization. However, existing systems often rely on a single data provider, such as movement sensors, cameras, or accelerometers, each with its limitations, leading to less than 100% reliability. Additionally, thereisanoticeablegapinexpertiseandsystematicknowledgeto

effectivelyintegratethesecomponents into arobust, user-friendly, and efficient system. The primary objective is to eliminate false alarms, ensuring accurate fall detection without disrupting the dailyliving patterns of the elderly. Falls pose as ignificant threat to the health of older individuals, with approximately one in three people over 65 experiencing at least one fall per year. These falls contribute to 90% of hip and wrist fractures and 60% of head injuries, not to mention the development of a fall ingamong many older individuals. Recent advancements in wireless communication and physiological sensing have led to the

development of small wearable devices, running on low battery power, for patient health monitoring in pervasive healthcare systems. These devices, strategically placed on key areas of the human body, can form a Body Sensor Network (BSN) connected by a wireless network. Also known as Wireless Body Area Networks, BSNs play a crucial role in pervasive healthcare, with the potential to revolutionize healthcare monitoring in diverse environments.

II.EXISTINGSYSTEM

The research presented in this study demonstrates significant benefits for critical patients, including those in comas, undergoing dialysis, or experiencing extended bedridden periods. In such conditions, even minor movements by the patient play a crucial role in their treatment. Unlike older systems that lacked techniques to detect patient movements accurately, this research introduces the use of sensors, enabling easy and efficient monitoring of patient activities. In the old method, the tracking of handgestures was not accurate, and for using health monitoring systems, a separate power supply was required, leading to increased consumption. Additionally, the accuracy of fall detection predictions was less reliable. The advancements proposed in this research address these shortcomings, paving the way for improved precision in tracking hand gestures, reducing the need for a separate power

supply, and enhancing the accuracy of fall detection predictions.

III.PROPOSED SYSTEM

Thissuggested method'sfirst step istesting itusing syntheticdata to determine important parameters and assess its efficacy against established approaches in the literature. The outcomes of change detection with real data, as well as the results of parameter extraction and selection, will then be shown. It is important to note that the accelerometer is used to distinguish between the positions of falling and lyingdown. Additionally, a gesture-based wheelchair control system and assistance device designed especially for older people living independently relies heavily on the Low Power Assist Device.Features like fall warnings, wheelchair gestures controlled by the patient, patient data measuring capabilities, and remote monitoring are all part of this integrated network. Every sensor is set up with a sample rate connected to the analog channel to guarantee accurate health parameter computation. The bare minimum of samples required for an effective computation is specified in the recommendations for the health monitoring index. When an alarm occurs, amessage is sent to the remote service center, which prompts a medical monitoring group to get in touch with the user and determine whether help is needed.

IV.MODULEDESCRIPTION

A. WristbandModule:

Description: The wristband module serves as the user interface, capturing motion and gesture inputs from the paralyzed patient. It is equipped with sensors and communication capabilities to transmit control signals wirelessly to the wheelchair control unit.

B. CommunicationModule:

Description: The communication module facilitates the transmission of data between the wristband and the wheelchair control unit. It ensures reliable, low-latency communication to provide real-time control over the wheelchair.

C. WheelchairControlUnit:

Description: The wheelchair control unit processes the signals received from the wristband module and translates them into specific wheelchair movements. It also manages safety features, power distribution, and overall control logic.

D. UserInterfaceModule:

Description: The user interface module provides feedback to the user, enhancing the overall user experience. It may include visual indicators, sound signals, or a display to convey information about wheelchair status, battery level, and system alerts.

E. PowerManagementModule:

Description: The power management module plays a crucial

role in maximizing the utilization of energy resources within the system. Its functions include monitoring battery levels, implementing energy-saving strategies, and ensuring the effective distribution of power.

F. SafetyModule:

Description: The safety module is designed to prevent accidents and enhance user safety during wheelchair operation. It includes features such as obstacle detection, collision avoidance, and an emergency stop mechanism.

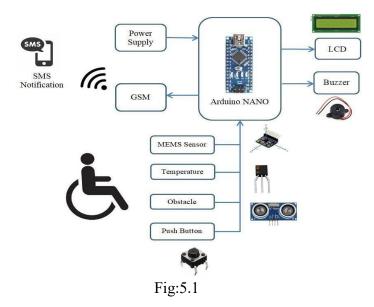
G. SecurityModule:

Description: The security module safeguards the communication between the wristband and the wheelchair control unit, preventing unauthorized access and ensuring the privacy of user data.

H. IntegrationModule:

Description: The integration module ensures the seamless collaboration of all systemcomponents.Itoverseestheinteraction

betweenthehardwareandsoftwareelements,fosteringacohesiveand well-functioning system. V.SYSTEMFLOWDIAGRAM



VI.SYSTEMTESTINGANDIMPLEMENTATION

The system testing and implementation for an IoT-based wristband-controlled wheelchair for paralyzed patients involve a systematic approach to ensure its reliability and functionality. with thorough analysis of requirements, the Beginning a process includes the design of a scalable system architecture, development of а prototype, and communication testing to verify data integrity and reliability. Subsequent functionality testing covers key aspects such as speed and direction control, emergency stop functionality, and obstacle detection. User interface and safety features are tested to guarantee usability and protection for users. Integration testing assesses theseamless operationof hardware andsoftware components, while battery and power management are optimized to extend device life. Network security testing is crucialtosafeguardcommunication, and user acceptance testing involving paralyzed patients helps ensure the system's user- friendliness. Comprehensive documentation, including user adherence manuals, troubleshooting guides, and to regulatory standards, is prepared before deployment. Continuous feedback and iteration based on realworldusagecontributetorefiningthe system's design and functionality, ultimately delivering a safe and reliable IoT-based wheelchair tailored to the needs of paralyzed patients.

VII.RESULTANDDISCUSSION

The implementation of the IoT-based wristband-controlled wheelchair for paralyzed patients has yielded promising results, demonstrating a viable solution for enhancing mobilityandindependenceamongindividuals with paralysis. The system underwent rigorous

testing, encompassing various aspects such as communication reliability, functionality, user interface, safety features, and network security. The communication between the IoT wristband and thewheelchaircontrolunitprovedtoberobust, with minimal latency and consistent data integrity. This ensures that users can control the wheelchair seamlessly using the wristband, promoting efficient and real-time responsiveness.Functionality testing revealed successful outcomes in terms of wheelchair control, encompassing forward, backward, left, and right movements, as well as speed adjustments and emergency stop functionalities. The user interface was found to be user-friendly, allowing easy navigation and control for paralyzed patients. The feedback provided to users, whether through visual indicators or auditorysignals, wasclearandunderstandable, enhancing the overall usability of the system.Safety features, including obstacledetectionandcollisionavoidancemechanisms, were effective in preventing potential accidents. The emergency stop functionality exhibited rapid response times, adding an extra layer of safety to the wheelchair operation. The integration of hardware and software components worked seamlessly, ensuring the cohesive operation of the entire system. Battery and power management optimizations contributed to an extended battery life, enhancing the overall sustainability and practicality of the IoT-based wheelchair.Network security measures implemented in the system proved effective in safeguarding communication between the wristband and the wheelchair control unit. This is crucial for maintaining the privacy and security of users, preventing unauthorized access or interference. User acceptance testing involving paralyzed patients provided valuable insights into the system's practicality and user- friendliness in real-world scenarios.

VIII.CONCLUSION

This study describes a low-cost gesture-operated smart wheelchair system designed to improve safety and enable pleasant wheelchair travel for those with severe impairments. Obstacle detection, fall detection, and an emergency messaging system are important safety features.Humantrialswereusedinthefirmwaredevelopmentprocess

to include both genuine ADXL sand simulated falls into the prototype.

Thedatasetsthatweregatheredweresplitbetweentrainingandtesting the fall classifier. In light of the fact that pressure is a major power- hungry component of the fall detection system, future research will look at better energy-efficient ways to gather and interpret pressure data. Fix-point computations will also improve coding efficiency by replacing floating-point calculations. Notably, rather than utilizing an older dataset, the reviewed fall detection system was created and evaluated using datasets from young volunteers.

IX.FUTUREWORK

Explore the integration of additional safety features into the wheelchair and wristband system. This could include fall detection sensors, collision avoidance technology, and real-

time monitoring of vital signs such as heart rate and blood pressure. Enable seamless integration with smart home systems to allow paralyzed patients greater independence and control over their environment. This could involve voice-activated commands to control lights, temperature, and other home appliances directly from the wristband.

X.REFERENCE

1]. Alshurafa N, Eastwood JA, Nyamathi S, Liu JJ, Xu W, Ghasemzadeh H, Pourhomayoun M, Sarrafzadeh M. Improving compliance in remote healthcare systems through smartphone battery optimization.IEEEJournalofBiomedicalandHealthInformatics.2014 Jun 9;19(1):57-63.

[2]. Yuan J, Tan KK, Lee TH, Koh GC. Power-efficient interruptdrivenalgorithmsforfalldetectionandclassification activities of daily living. IEEE Sensors Journal. 2014 Sep 18;15(3):1377-87.

[3].J.Singha,S.Misra,andR.H.Laskar, "Effectofvariation

ingesticulationpatternindynamichandgesturerecognition system," Neurocomputing,vol. 208, pp. 269-

280,Oct.2016,doi:10.1016/j.neucom.2016.05.049.

[4]. Y. Rabhi, M. Mrabet, F. Fnaiech, P. Gorce, I. Miri, and C. Dziri, "Intelligent touchscreen joystick for controlling electric wheelchair," Irbm, vol. 39,no. 3, pp. 180–193, Jun. 2018, doi: 10.1016/j.irbm.2018.04.003.

5]. Bianchi F, Redmond SJ, Narayanan MR, Cerutti S, Lovell NH. Barometric pressure and triaxial accelerometry-based falls event detection.IEEE Transactionson Neural Systems and Rehabilitation Engineering. 2010 Aug 30;18(6):619-27.

6]. H.-S. Grif and T. Turc, "Human hand gesture based system for mouse 587 cursor control," Proc. Manuf., vol. 22, pp.1038–1042, Jan. 2018, doi:5810.1016/j.promfg.2018.03.147.

[7]. A. Skraba, A. Kolozvari, D. Kofjac, and R. Stojanović, "Wheelchair553maneuveringusingleapmotioncontroller and cloud based speech 554 control: Prototype realization," in Proc. 4th Medit.Conf. Embedded 555 Comput. (MECO), Jun. 2015, pp. 391–394, doi:10.1109/MECO.2015. 556 7181952.

[8]. S. Song, D. Yan, and Y. Xie, "Design of control system based onhand 583 gesture recognition," in Proc. IEEE 15th Int. Conf. Netw.,Sens. Con584trol(ICNSC), vol. 16, Mar. 2018, pp. 1–4, doi:10.1109/ICNSC.2018. 585 8361351.

Lamb Madhe. "Automatic [9]. Κ. and S. bed position control basedonhand489gesturerecognitionfordisabledpatients,"in Proc. Int. Conf. Autom. 490 Control Techn. (ICACDOT), 2016, 148-153. 491 Dyn. Optim. Sep. pp. doi: 10.1109/ICACDOT.2016.7877568.

[10]. J. W. Machangpa and T. S. Chingtham, "Head gesture controlled 497 wheelchair for quadriplegic patients," Proc. Comput. Sci., vol. 132, 498 pp. 342–351, Jan. 2018, doi: 10.1016/j.procs.2018.05.189.

[11]. Y. M. Jain, S. S. Labde, and S. Karamchandani, "Gesture controlled 500 wheelchair for quadriplegic children," in Proc. 3rd Int. Conf. Syst. Inform. 501 (ICSAI), Nov. 2016, pp. 121–125, doi: 10.1109/ICSAI.2016.7810941.

[12]. Y. Rabhi, M.Mrabet, andF. Fnaiech, "Optimized joystick control inter- 503 face for electric powered

wheelchairs," in Proc. 16th Int. Conf. Sci. 504 Techn. Autom. Control Comput. Eng. (STA), Dec. 2015, pp. 201–206, doi: 505 10.1109/STA.2015.7505092.

[13].Y.Rabhi,M.Mrabet,F.Fnaiech,P.Gorce,I.Miri, and

C. Dziri, "Intelligent 507 touchscreen joystick for controlling electric wheelchair," IRBM, vol. 39, 508 no. 3, pp. 180–193, Jun. 2018, doi: 10.1016/j.irbm.2018.04.003.

[14].R.K.Megalingam,S.Sreekanth,A.Govardhan,C.R.

Teja,and510A.Raj,"Wirelessgesturecontrolled wheelchair," in Proc. 4th Int. 511 Conf. Adv. Comput.

Commun.Syst.(ICACCS),Jan.2017, pp.3–7, doi: 512 10.1109/ICACCS.2017.8014621.

[15].A. Haria, A. Subramanian, N. Asokkumar, S. Poddar, and J. S. Nayak, 514 "Hand gesture recognition for human computer interaction," 515 Proc. Comput. Sci., vol. 115, pp. 367–374, Jan. 2017, doi: 516 10.1016/j.procs.2017.09.092.

[16]. U. V. Solanki and N. H. Desai, "Hand gesture based remote control for 518 home appliances: Handmote," in Proc. WorldCongr.Inf.Commun.Tech-519nol.,Dec.2011,pp. 419–423, doi: 10.1109/WICT.2011.6141282.

[17]. M. S. Verdadero, C. O. Martinez-Ojeda, and J. C. D. Cruz, "Hand ges- 521 ture recognition system as an alternative interface for remote controlled 522 home

appliances," in Proc. IEEE 10th Int. Conf. Humanoid, Nanotechnol., 523 Inf. Technol., Commun. Control, Environ. Manag. (HNICEM), Nov. 2018, 524 pp. 1–5, doi: 10.1109/HNICEM.2018.8666291.

[18]. S. Nasif and M. A. G. Khan, "Wireless head gesture controlled 526 wheel chair for disable persons," in Proc. IEEE Region 10 527 Humanitarian Technol. Conf. (R10- HTC), Dec. 2017, pp. 156–161, 528 doi: 10.1109/R10- HTC.2017.8288928.

[19]. H. Cheng, L. Yang, and Z. Liu, "Survey on 3D hand gesture recognition," 530 IEEE Trans. Circuits Syst. Video Technol., vol. 26, no. 9, pp. 1659–1673, 531 Sep. 2016, doi: 10.1109/TCSVT.2015.2469551.

[20]. K. Sadeddine, F. Z. Chelali, R. Djeradi, A. Djeradi, and 658 S. Benabderrahmane, "Recognition of user-dependentand independent 659 static hand gestures: Application to sign language," J. Vis. Commun. 660 Image Represent., vol. 79, Aug. 2021, Art. no. 103193, doi: 661 10.1016/j.jvcir.2021.103193.